

Development of a nanoemulsion incorporating 3-acetyl-11-keto- β -boswellic acid (AKBA): Solubility and oral bioavailability through in vitro and in vivo studies

Najmeh Ketabchi

Tehran University of Medical Sciences

Seyed Nasser Ostad

Tehran University of Medical Sciences

Mahmoud Ghazi-Khansari

Tehran University of Medical Sciences

Hossein Ghanbari

Tehran University of Medical Sciences

Fariba Esmaeili

Tehran University of Medical Sciences

Amir Amani

a.amani@nkums.ac.ir



North Khorasan University of Medical Sciences

Research Article

Keywords: Drug delivery, Nanoemulsion, AKBA, boswellic acid, pharmacokinetics, bioavailability permeability

Posted Date: November 3rd, 2025

DOI: <https://doi.org/10.21203/rs.3.rs-7838340/v1>

License:   This work is licensed under a Creative Commons Attribution 4.0 International License.
[Read Full License](#)

Additional Declarations: No competing interests reported.

**Development of a nanoemulsion incorporating 3-acetyl-11-keto- β -boswellic acid (AKBA):
Solubility and oral bioavailability through in vitro and in vivo studies**

Najmeh Ketabchi¹; Seyed Nasser Ostad²; Mahmoud Ghazi-Khansari³; Hossein Ghanbari¹;
Fariba Esmaeili¹; Amir Amani^{*,4,5}

¹ Department of Medical Nanotechnology, School of Advanced Technologies in Medicine,
Tehran University of Medical Sciences, Tehran, Iran

² Toxicology and Poisoning Research Center, Department of Toxicology and Pharmacology,
Faculty of Pharmacy, Tehran University of Medical Sciences, Tehran, Iran.

³ Department of Pharmacology, School of Medicine, Tehran University of Medical Sciences,
Tehran, Iran

⁴ Natural Products and Medicinal Plants Research Center, North Khorasan University of
Medical Sciences, Bojnurd, Iran

⁵ Department of Advanced Technologies, School of Medicine, North Khorasan University of
Medical Sciences, Bojnurd, Iran

Corresponding author:

a.amani@nkums.ac.ir, Tel/fax: +98-58-32297097

21 **Abstract**

22 **background:** 3-Acetyl-11-keto- β -boswellic acid (AKBA) has attracted considerable interest due
23 to its therapeutic potential against inflammatory and cancer-related disorders. However, its
24 poor oral bioavailability remains a critical limitation for clinical application. This study aimed
25 to enhance the bioavailability of AKBA by developing a nanoemulsion (NE)-based delivery
26 system.

27 **Results:** Several NE formulations were optimized and characterized based on drug loading,
28 stability, and droplet size. The optimized NE-AKBA showed a particle size of 12–15 nm and was
29 further tested for permeability across Caco-2 cell monolayers, followed by in vivo
30 pharmacokinetic evaluation. Permeability studies revealed significantly improved transport of
31 NE-AKBA within the first hour. Pharmacokinetic analysis indicated a notable increase in
32 systemic exposure: the C_{\max} of AKBA rose from 3.36 to 12.23 $\mu\text{g/mL}$, while the AUC_{0-t} increased
33 from 4257 to 6222 $\mu\text{g}\cdot\text{h/mL}$, with T_{\max} remaining steady at 6 hours.

34 **Conclusion:** These findings demonstrate that nanoemulsion-based delivery significantly
35 improves the oral bioavailability of AKBA and provides a promising platform for its future
36 therapeutic development.

37

38 **Keywords:**

39 Drug delivery; Nanoemulsion; AKBA; boswellic acid; pharmacokinetics; bioavailability
40 permeability

Background

3-Acetyl-11-keto- β -boswellic acid (AKBA) is a bioactive compound of *Boswellia serrata* gum resin, a plant known for its potent anti-inflammatory activity. AKBA has exhibited great therapeutic potential in the management of chronic inflammatory diseases such as rheumatoid arthritis [1], osteoarthritis [2], asthma, and inflammatory bowel disease (IBD) [3], neurodegenerative disorders [1, 4], chronic colitis [5], and cancers [6-8]. However, despite their therapeutic potential, there are significant challenges to their bioavailability due to their physicochemical properties. As a Biopharmaceutical Classification System (BCS) Class II drug, AKBA is poorly soluble in water ($<1\text{ }\mu\text{g/mL}$) but highly permeable [9]. Its high lipophilicity ($\log P = 3.3$) and extensive first-pass metabolism in the gut and liver also limit its systemic availability, resulting in low bioavailability [10, 11]. These limitations have driven the demand for new drug delivery systems to optimize their therapeutic effects. The structure of AKBA is schematically shown in Figure 1.

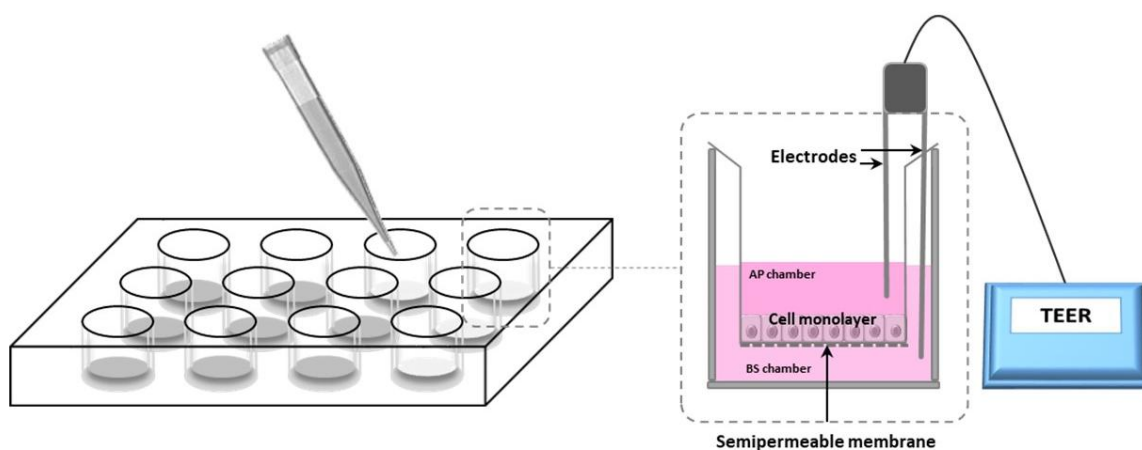


Figure 1. Schematics of the insert plate and its components used during the experiment.

The test samples were then added to the AP side and maintained in an incubator. TEER was measured after 1, 2, and 3 hours to calculate the cell permeability for AKBA. All AP and the

last BP media were taken, and their absorbance was measured at 249 nm for the determination of AKBA values [12].

Various drug delivery carriers, such as liposomes, nanomicelles, dendrosomes [13], nanostructured lipid carriers (NLCs) [14], and solid lipid nanoparticles (SLNs) [13] have been explored to overcome these challenges. Nanoemulsions (NEs) have emerged as highly effective and versatile options because of their simple formulation, stability, and enhanced drug solubility and permeability [15]. NEs are composed of two immiscible liquids stabilized with surfactants, forming nanoscale droplets that enhance the dispersion of hydrophobic compounds in aqueous media [16, 17]. They possess a small droplet size and stability, owing to which they are ideal for the delivery of poorly soluble drugs such as AKBA [18]. Furthermore, NEs also enhance drug absorption via diverse mechanisms involving an increase in the fluidity of the cell membrane, increased transcellular and paracellular transport, and increased uptake into the lymph [16, 17, 19, 20]. All these factors make NEs promising carriers that can improve the bioavailability of AKBA.

Recently, advances in NE technology have been the driving force behind the development of the best cosurfactants, surfactants, and oil phases to establish stable and efficient drug delivery systems. The use of multiple surfactants and cosurfactants has been found to improve the stability of NE and reduce its droplet size by optimizing the hydrophilic–lipophilic balance (HLB) [21–23]. Owing to their unique molecular architecture, cosurfactants enhance interfacial fluidity and promote the formation of stable nanoemulsions at lower concentrations of surfactants, limiting potential toxicity [24, 25]. Similarly, the choice of the oil phase is also an essential consideration in determining the stability, droplet size, and activity of NEs. Oils with

low water solubility can inhibit Ostwald ripening, whereas blended oils can maintain unimodal droplet size distributions, both of which increase stability [26, 27].

Recent studies have shown the capacity of long-chain fatty acid (LCFA) oils to improve lipophilic drug bioavailability. For example, a study on simvastatin-loaded NEs revealed improved oral bioavailability by a significant percentage through better lymphatic absorption via LCFA-based lipids [26]. Based on these results, this study aimed to prepare AKBA-loaded NEs from natural LCFA oil to increase the bioavailability of AKBA. Given the distinct advantages of NEs and their ability to modify their formulation compositions, this research attempts to overcome the bioavailability limitations of AKBA, raising hope for widespread therapeutic use in the future.

Methods

AKBA was purchased from Baoji Herbest Bio-Tech Co. (China). Olive oil, coconut oil, almond oil, and sesame oil were purchased from Farabi Pharmaceutical Co. (Iran). Tween 80 and Span 80 (Lab reagent grade) were purchased from Central Drug House Ltd. (India). Chloroform, acetone, and methanol (absolute) were from NeutroChrom® (Iran). Caco-2 cells were obtained from Pasteur Institute of Iran> DMEM (5,000 mg/L d-glucose, 100 mg/L sodium pyruvate, and l-glutamine) and fetal bovine serum (FBS) were from Bioidea (Iran). T-25 cm² treated culture flasks were from SPL-Biosciences®, and cell culture filter inserts (24-well transwell Culture Plate) were obtained from SPL® (Korea).

Nano-emulsion preparation

Different NE preparations were prepared using different contents of Tween 80 (Polyoxyethylene 20 monooleate) [18, 28], Span 80 (Sorbitan monooleate) [18], edible oil (olive oil, coconut oil, sesame oil, or almond oil), and co-surfactant (ethanol, propylene glycol, sorbitol, or glycerol) by mixing surfactants and oil on a magnetic stirrer for 20 minutes, then adding co-surfactant and titrating with water [18]. The selection of surfactant concentration was performed using the hydrophilic-lipophilic balance (HLB) value [29]. After achieving the optimized formulation in terms of its transparency, physical stability, and droplet size distribution, AKBA was loaded in the NE by being dissolved in the oil phase during the preparation of NE (NE-AKBA).

Stability tests

Accelerated tests of physical stability were used to investigate the stability of the prepared NE. In this way, the samples were placed periodically in harsh conditions (cooling-heating cycles and centrifuge), then their stability was evaluated in terms of appearance (transparency and phase separation) as well as the size of the particles [18].

Droplet size, size distribution, and zeta potential

The mean particle size and polydispersity index (PDI) of NE-AKBA were measured by dynamic light scattering (DLS) at ambient temperature. Due to the thickness of the samples, each sample was diluted up to three times before measuring the size of the particles. The zeta potential was determined using a Zetasizer by electrophoretic mobility under an electric field.

Transmission electron microscopy

The morphology and size of the NE nanoparticles were confirmed using transmission electron microscopy (TEM) (LEO 906, Zeiss, Germany). A drop of an aqueous solution of

phosphotungstic acid was added as negative staining on the grid, and the staining was performed for 5 min at room temperature. The prepared sample was then evaluated by TEM at a voltage of 200 kV.

In vitro studies: Cell Viability Assay

The cytotoxicity of AKBA and NE-AKBA was evaluated using the MTT assay. Caco-2 cells were cultured in T-25 cm² treated culture flasks in high-glucose DMEM (5,000 mg/L d-glucose, 100 mg/L sodium pyruvate, and L-glutamine), supplemented with 20% FBS. The flasks were maintained at 37 °C in a CO₂ incubator with atmospheric air kept at 95% air and 5% CO₂ at 95% humidity and supplied with fresh medium every 2 days until they reached approximately 80% confluence in 5–7 days. Cell cultures at passage 23 were detached with Trypsin–EDTA, then seeded at 1×10^3 cells/well in 96-well plates [30, 31]. Three days after seeding, the wells were grouped and treated with 1) NE-AKBA (nanoemulsion containing AKBA), 2) NE (nanoemulsion without AKBA), 3) AKBA (bulk AKBA suspension in water), and 4) control group (no treatment). Six hours later, the medium was removed from the wells, and MTT reagent was added to the wells (5 mg mL⁻¹ stock). The plates were incubated for 3 h in the incubator and lysed with DMSO (100 µL per well). The absorbance of the wells was measured using an ELISA microplate spectrophotometer at 570 nm [32, 33]. The obtained OD values were normalized to the blank wells, and the Caco-2 cell viability was evaluated. Afterward, using a graphical method and linear regression, the IC₅₀ (half maximal inhibitory concentration) of NE-AKBA in Caco-2 cells was calculated [34].

Trans-epithelial electrical resistance (TEER) assay

Transport was determined across Caco-2 cell monolayers in the apical-to-basolateral direction [35]. Cells were seeded on cell culture filter inserts (50,000 cells/well). Culture medium

(DMEM) was added to the apical (AP) (300 µL) and basolateral (BL) (600 µL) sides, and the plate was kept at 37°C in a humidified incubator containing 5% CO₂ in air. DMEM was replaced every other day for the first week and once a week thereafter. Cells were left to differentiate for 18–21 days [36, 37]. The trans-epithelial electrical resistance (TEER) value was measured weekly to assess cell differentiation and monolayer formation.

After equilibration at room temperature, the TEER was measured in HBBS medium (Hanks' balanced salt solution). The treatments were added to the AP compartment without changing the BS environment. A pair of chopstick electrodes that reported resistance values was inserted in the AP and BL chambers, and the TEER values were recorded (Figure 1). TEER values ranging from 200 to 600 Ohms per cm² of the porous membrane were considered as indicators of an integrated monolayer, while TEER values < 200 Ohms indicated loss of integrity; thus, the setup was excluded from the experiments [29].

The apparent permeability (P_{app}) coefficient (cm/s) was calculated as below:

$$P_{app} = \frac{V_R}{A \times C_0} \times \frac{dQ}{dt}$$

Where V_R is the volume in the BL chamber (mL), A is the surface area of the porous cup (cm²), C_0 is the initial drug concentration (µg/mL), and dQ/dt is the initial slope of the cumulative concentration (µg/mL) in the BL chamber with time (seconds) [38].

In-vivo studies

The pharmacokinetics of the NE-AKBA were studied in female white Wistar rats weighing 200 – 250 g, supplied by the Department of Pharmacology of Tehran University of Medical Sciences (Iran). For blood sample collection, rats were housed in standard laboratory cages for several days before experimentation to allow acclimatization to the environmental conditions.

168 During this period, the animals were gradually habituated to gentle handling and restraint
169 procedures to minimize stress during sampling. The rats were housed under standard
170 conditions with a standard pellet diet, water ad libitum, and 12-hour light and dark cycles.
171 They were grouped randomly into two groups, consisting of four rats, and each group was
172 gavaged with 1 ml of either NE-AKBA or AKBA suspension (1 mg/ml). Then, each rat's tail was
173 warmed individually using a heating pad at approximately 37–40 °C and gently massaged to
174 facilitate vasodilation. Subsequently, 200 µL of blood was collected from the lateral tail vein
175 using an insulin syringe equipped with a 25–27 G needle. At each sampling time point, blood
176 was withdrawn from the opposite side of the tail relative to the previous collection, and the
177 puncture site was shifted 2–3 mm distal to the prior site to prevent repeated injury to the
178 same location.

179 At the end of the 48-hour sampling period, rats were anesthetized with a ketamine/xylazine
180 mixture prepared at a 10:1 ratio (total administered volume 0.45 mL per animal). After
181 achievement of a surgical plane of anesthesia, a terminal cardiac puncture was performed to
182 obtain the final blood sample. Following exsanguination, an additional intraperitoneal
183 injection of ketamine was administered to ensure death, consistent with the study's
184 institutional animal care and use committee (IACUC)-approved protocol.

185 Rat blood samples were collected at 1, 2, 3, 6, 12, 24, and 48 h after gavage. The samples were
186 centrifuged for 20 min at 2000 rpm to obtain the plasma and treated with acetone (1.5:1) to
187 remove the proteins, and centrifuged (15 min, 3000 rpm). The supernatant was extracted with
188 chloroform (2:1). The solvent was then removed, and the dry residue was dissolved in
189 methanol and analyzed using a Cytation3 Imaging reader (Biotek, USA) at 249 nm [39, 40].
190 The maximum concentration (C_{\max}) of AKBA in the plasma and the time to reach the maximum

concentration (T_{\max}) were obtained from the observed values. The area under the concentration-time curve (AUC_{0-t}) was then calculated. An unpaired Student's t-test was conducted for significance evaluation with p-value < 0.05.

Results

Preparation and characterization of nanoemulsion

Table 1 shows the properties of selected prepared NEs. From the accelerated stability tests, the optimum NE preparation was determined as having 3% oil, 30.3% Tween 80, 7.7% Span 80, and 10% ethanol in deionized water. Table 2 shows the DLS results of the optimum NE preparation. Our results also indicated that the NE exhibits Newtonian behavior. The Zeta potential of the NE-AKBA was -14.5 mV.

The droplet's morphology was observed by TEM microscopy and showed a spherical shape with a particle size of ~20 nm, close to that of DLS results (see Figure 2).

Table 1. Composition, stability, particle size, and maximum AKBA solubility of selected nanoemulsion preparations

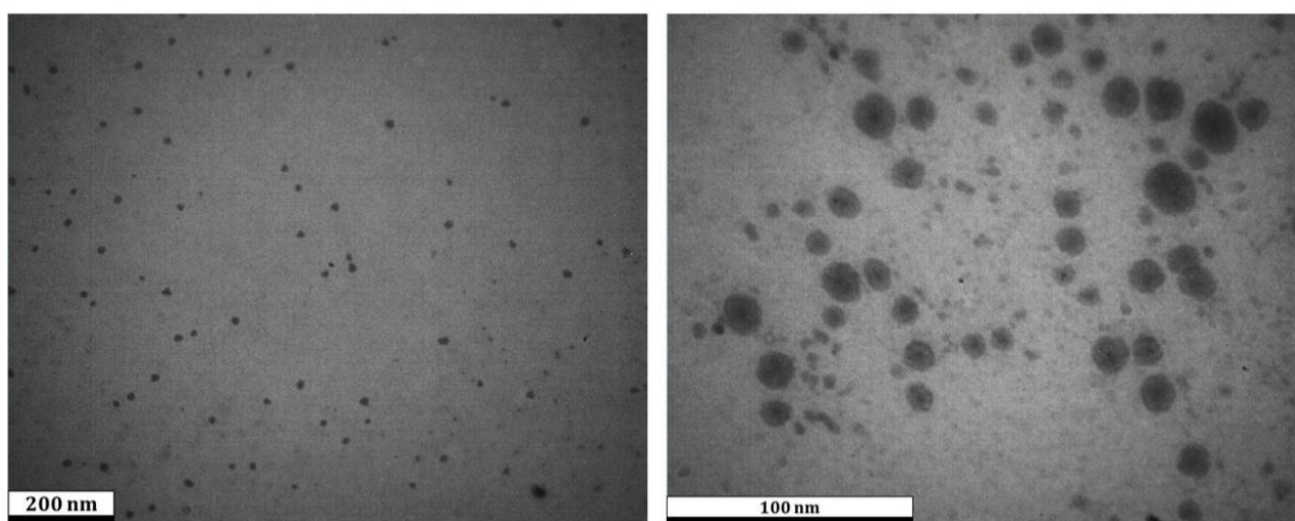
Oil type	Oil (%)	Span 80 (%)	Tween 80 (%)	Ethanol (%)	Surfactant (%)	water (%)	Surfactant & Cosurfactant. (%)	Stability at room temperature	Particle size (nm)	AKBA in NE (%)
Olive	2	4.2	30.8	9	35	54	44	≤ 1 month	23.2	0.064
Sesame	3	6.2	29.8	10	36	51	46	≤ 1 month	18.1	0.105
Coconut	4	5.9	28.1	12	34	50	46	≥ 1 year	15.1	0.076
Coconut	4	6.1	28.9	12	35	49	47	≤ 6 months	18.6	0.076
Coconut	3	4.9	30.1	12	35	50	47	≥ 1 year	19.3	0.057
Almond	3	7.5	29.5	10	37	50	47	≤ 1 month	12.8	0.120
Almond	3	7.7	30.3	10	38	49	48	≥ 1 year	14.3	0.120

205

Table 2. DLS results of NE-AKBA

	Day 1	Day 7	Day 30	Month 6	Month 12	Month 15	Centrifuged	Freeze-thawed
d50	8.3	8.2	12.1	14.3	15.1	14.7	11.9	23.8
Observed peaks	1	3	3	3	3	3	2	2
Viscosity (cp)	0.8132	0.8144	0.8497	0.8317	0.8320	0.8319	0.8678	0.8497

206



207

208

Figure 2. TEM images of nanoemulsion containing AKBA

209 In-vitro results

210 To determine the toxicity of AKBA and NE-AKBA on Caco-2 cells, an MTT assay was performed.

211 The IC₅₀ value of AKBA was found as 0.025 μ M for NE-AKBA and 1.615 μ M for AKBA (Figure

212 3-a). From the MTT findings, the maximum tolerable concentration of NE-AKBA was obtained

213 as 1.29×10^{-7} μ g/ml. So, 1 μ g/ml was then used to treat the Caco-2 cells. For TEER studies. From

214 Figure 3-b (which shows the TEER value after cell seeding), from day 21 onwards, the TEER

215 value was more than 200 Ohms per cm^2 , indicating the formation of an integrated monolayer

216 [29] (Figure 3-b).

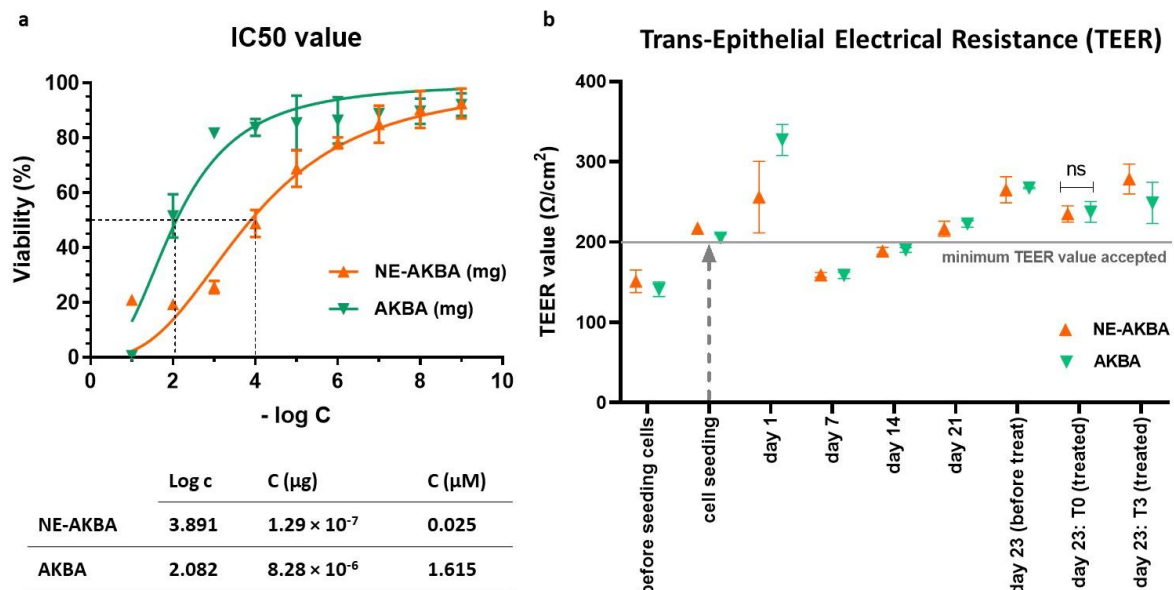


Figure 3. a) viability percentage of Caco-2 cells exposed to AKBA and NE-AKBA at different doses. b) TEER value changes during the permeability assay (from washing the inserts with media until 3 h after treatment)

From the permeability studies (see Figure 4), AKBA tends to accumulate in the BL side of the monolayer. The increase appears to be linear in the bulk AKBA treatment. Additionally, after the first hour, the increase in the NE-AKBA-treated group had a similar slope to that of the bulk AKBA-treated group. Apparent permeability coefficient (P_{app}) was calculated, and as shown in Figure 5, it is significantly higher in the NE-AKBA group.

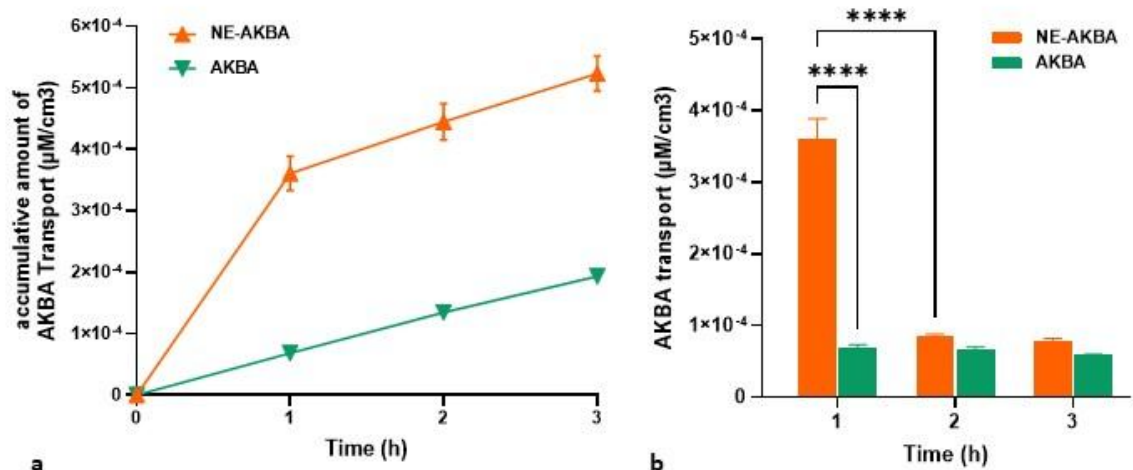


Figure 4. a) cellular transport of AKBA from NE-AKBA and free AKBA. Both treatments were added to the AP side of the Caco2 cell, and samples were taken from the BA sides at 1, 2, and 3 h post-treatment. Results are expressed as percent of the initial dose (n = 3). b) Effect of AKBA and NE-AKBA treatment on the permeability of treated Caco-2 cells. Caco-2 monolayers grown on culture inserts were treated with AKBA and NE-AKBA (C=2 μg/ml) for 3

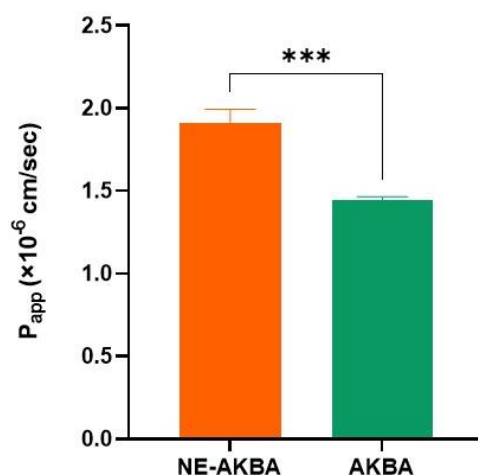
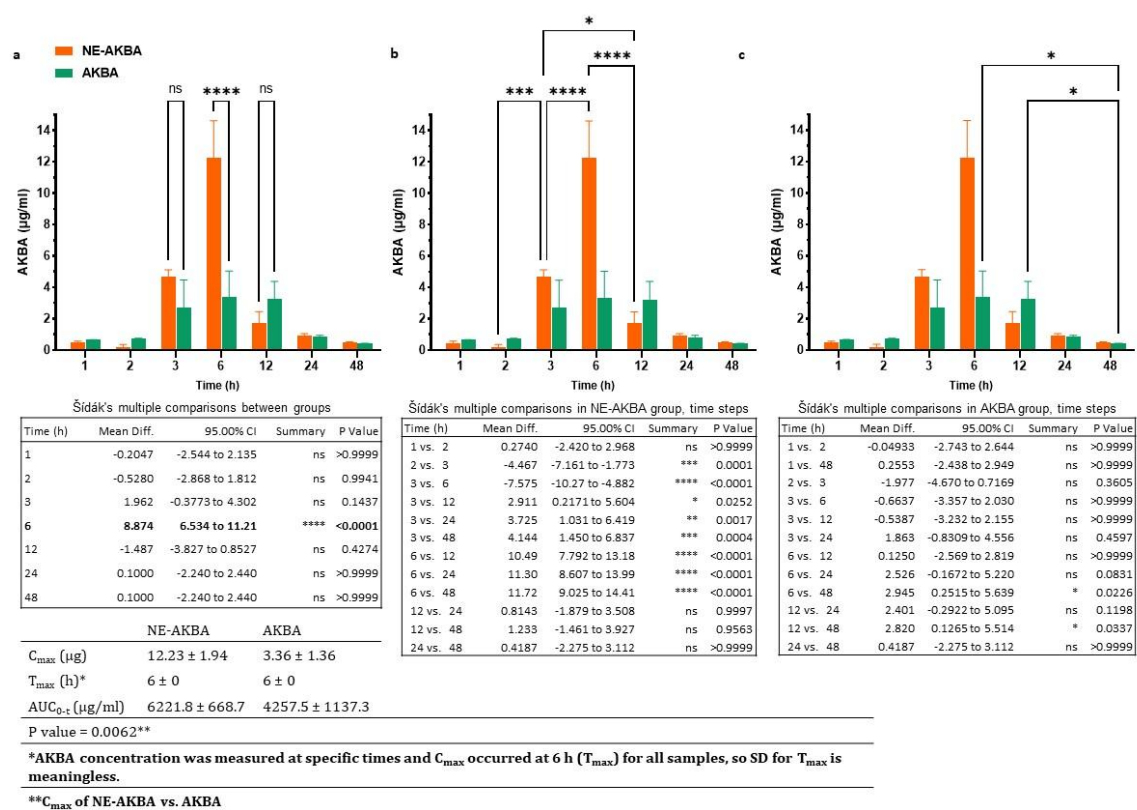


Figure 5. permeability of Caco-2 cells for AKBA released from NE-AKBA and AKBA in 3 h post-treatment; Means ± S.D., n = 3; ***p < 0.001. P_{app} is an apparent permeability coefficient.

238 **In-vivo results**

239 The amount of AKBA in the plasma samples of the rats that were treated with either AKBA or
240 NE-AKBA (1mg/kg, one dose) was measured at different time points after sampling. The
241 highest concentration of AKBA in the plasma (C_{max}) and the time to reach this maximum
242 concentration (T_{max}) were measured. Then, the surface area below the curve was calculated
243 as AUC_{0-T} (see Figure 6). From the details, a significant increase in C_{max} and AUC_{0-T} of NE-AKBA
244 is observed compared with AKBA. As evident, at time 6 h (i.e., T_{max}), an important difference
245 is observed between the plasma concentration of AKBA in the two groups. It is also worth
246 mentioning that the standard deviation value for T_{max} reported in this study (i.e., zero) is due
247 to the sampling time points (i.e., 1, 2, 3, 6, 12, 24, and 48 h). In all experiments, the maximum
248 concentration was detected at time point 6; thus, the SD equaled zero in this study.



249

Figure 6. Mean (SD) AKBA amount in plasma samples per time (left). AKBA amounts ($\mu\text{g/ml}$) detected in plasma samples of rats (top right). C_{max} and T_{max} were obtained directly from the diagram (bottom right). AUC_{0-t} is the surface area under the curve. Differences between groups and times were calculated by Unpaired Student's t-test, *, **, *** indicate $p < 0.05$, $p < 0.01$, and $p < 0.001$, respectively.

Discussion

In this study, Tween 80 (a hydrophilic surfactant) and Span 80 (a hydrophobic surfactant) were employed to adjust the HLB of the system [41, 42]. Using different edible oils, transparent nanoemulsions (NEs) were prepared and evaluated for AKBA loading and stability. Among the oils tested, almond oil-based NE showed the smallest droplet size, the highest stability, and the greatest AKBA solubility. The optimized formulation remained stable at room temperature for over 15 months, demonstrating long-term storage potential.

Initially, TEER values were low due to the porosity of the insert plate membrane. Following cell seeding, TEER increased, likely due to suspended cells accumulating within the pores and gradually covering them. After one week, cells differentiated and adhered to the membrane and each other, forming tight junctions, which further increased TEER. A decrease in TEER was observed after changing the medium, likely due to the removal of dead or non-adherent cells [43].

On day 21, after confirming monolayer integrity via TEER measurements, cells were treated with AKBA and NE-AKBA, and results were compared with untreated controls. AKBA content in the basolateral (BL) chamber was assessed for three hours post-treatment to evaluate

272 permeability across the intestinal epithelial model. Both AKBA and NE-AKBA initially caused a
273 TEER reduction (T0), which recovered after three hours (T3). Cumulative AKBA transport
274 ($\mu\text{M}/\text{cm}^3$) was calculated to determine apparent permeability (Papp). NE-AKBA treatment
275 resulted in significantly higher AKBA transport during the first hour compared with later time
276 points. Unlike bulk AKBA, which exhibited a constant transport rate, NE-AKBA displayed a
277 biphasic transport pattern, characterized by accelerated transport during the first hour.

278 While the exact mechanism underlying this early increase in transport remains unclear, it may
279 relate to the known low-rate active transport of AKBA [44] and potential NE-mediated
280 enhancement of active uptake [45]. Additionally, smaller droplets (<100 nm) may facilitate
281 rapid intercellular passage, temporarily affect tight junction integrity, and reduce TEER in the
282 early stage [46-48]. These observations suggest that NEs can improve the intestinal
283 permeability of hydrophobic compounds such as AKBA through both intracellular and
284 paracellular pathways.

285 Pharmacokinetic evaluation in rats confirmed enhanced oral absorption of NE-AKBA. Plasma
286 concentrations of AKBA were significantly higher in the NE-AKBA group compared with bulk
287 AKBA, as indicated by increased C_{max} and AUC0-t. The low dose used in this study (1 mg/kg)
288 was chosen to minimize potential kidney toxicity associated with high levels of boswellic acids
289 (BAs) [49] and to reflect the efficiency of NE formulation. Literature comparisons show
290 variability in C_{max} and T_{max} , likely due to differences in *Boswellia* strains, resin composition,
291 dosage, analytical methods, or formulation strategies [50-53]. In our study, T_{max} remained
292 unchanged (6 h), consistent with prior reports [51].

293 The increase in AUC0-t (from 4257.5 ± 1137.3 to 6221.8 ± 668.7 $\mu\text{g}/\text{ml}$) confirms improved
294 AKBA bioavailability with NE formulation. This enhancement aligns with findings for other

295 lipophilic drugs such as *mebudipine* and atovaquone [54, 55] and is likely attributable to
296 improved solubility [56], modulation of biological barriers [57, 58], and/or enhanced
297 lymphatic transport through lipoprotein formation [59]. Overall, the results demonstrate that
298 nanoemulsion-based delivery is an effective strategy for improving the oral bioavailability of
299 poorly soluble compounds like AKBA.

300

301 **Conclusion**

302 This study demonstrated that encapsulating AKBA in a nanoemulsion significantly enhanced
303 its oral bioavailability. Both in vitro and in vivo findings confirmed an increased transport of
304 AKBA, potentially facilitated through intercellular pathways in Caco-2 cells. These results
305 highlight nanoemulsion-based delivery as a promising strategy for improving the therapeutic
306 efficacy of poorly soluble compounds such as AKBA.

307

308 **Declarations:**

309 **Ethics approval and consent to participate**

310 All techniques and experimental procedures were executed in strict adherence to the
311 pertinent regulations and directives set forth by the esteemed Ethical Committee of Tehran
312 University of Medical Sciences (approval code: IR.TUMS.VCR.REC.1398.212).

313

314 **Consent for publication**

315 Not applicable

316

317 **Availability of data and materials**

318 The datasets used and/or analyzed during the current study are available from the
319 corresponding author on reasonable request.

320

321 **Competing interests**

322 The authors declare that they have no competing interests

323

324 **Funding**

325 This project was supported by the Tehran University of Medical Sciences (grant number 98-
326 01-87-41850)

327

328 **Authors' contributions**

329 The individual contributions of the authors are as follows:

- 330 • Najmeh Ketabchi: Conceptualization, Investigation, Formal Analysis, Validation,
331 Visualization, Writing – Original Draft.
- 332 • Seyed Nasser Ostad: Supervision (specific oversight and guidance on drug selection
333 and properties).
- 334 • Mahmoud Ghazi-Khansari: Resources, Supervision (specific oversight and guidance on
335 in vitro studies).

- 336 • Hossein Ghanbari: Supervision (specific oversight and guidance on in vivo studies).
- 337 • Fariba Esmaeili: Methodology, Resources.
- 338 • Amir Amani: Conceptualization, Resources, Project Administration, Writing – Review
- 339 & Editing, Funding Acquisition, Supervision (overall supervision of the research, with
- 340 specific oversight on nanoemulsion preparation).

341 All authors have read and approved the final submitted version of the manuscript.

342

343 Acknowledgements

344 Not applicable

345

346 References

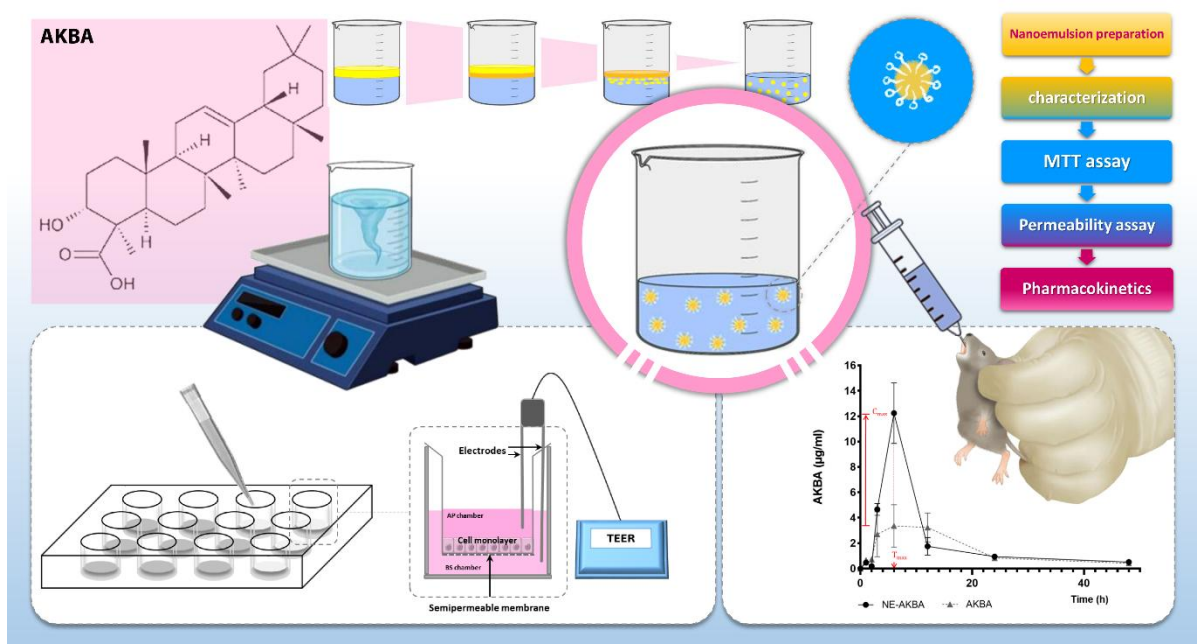
- 347 1. Gong Y, Jiang X, Yang S, Huang Y, Hong J, Ma Y, Fang X, Fang Y, Wu J: **The biological activity of**
- 348 **3-O-acetyl-11-keto- β -boswellic acid in nervous system diseases.** *Neuromolecular medicine*
- 349 2022, **24**(4):374-384.
- 350 2. Zhou J, Shao Z, Han Z, Qian Y, Xu M, Zhang D, Xu T, Yan K, Ge G, Tao H: **Acetyl-11-keto- β -**
- 351 **boswellic acid Restrains Inflammation and Extracellular Matrix Degradation of**
- 352 **Osteoarthritis via Suppression of NF- κ B Pathway.** 2022.
- 353 3. Zhang P, Jiang H: **Acetyl-11-keto- β -boswellic Acid Confers Protection in DSS-Induced Colitis**
- 354 **via the JNK-p38 MAPK and NF- κ B Signaling Pathways.** *Advanced Biology* 2023,
- 355 **7**(6):2200247.
- 356 4. Ding Y, Chen M, Wang M, Wang M, Zhang T, Park J, Zhu Y, Guo C, Jia Y, Li Y: **Neuroprotection**
- 357 **by acetyl-11-keto- β -boswellic acid, in ischemic brain injury involves the Nrf2/HO-1 defense**
- 358 **pathway.** *Scientific reports* 2014, **4**(1):7002.
- 359 5. Kriegelstein CF, Anthoni C, Rijcken EJ, Laukötter M, Spiegel H-U, Boden SE, Schweizer S, Safayhi
- 360 H, Senninger N, Schürmann G: **Acetyl-11-keto- β -boswellic acid, a constituent of a herbal**
- 361 **medicine from *Boswellia serrata* resin, attenuates experimental ileitis.** *International journal*
- 362 *of colorectal disease* 2001, **16**:88-95.
- 363 6. Gong C, Li W, Wu J, Li Y-Y, Ma Y, Tang L-W: **AKBA inhibits radiotherapy resistance in lung**
- 364 **cancer by inhibiting maspin methylation and regulating the AKT/FOXO1/p21 axis.** *Journal*
- 365 *of Radiation Research* 2023, **64**(1):33-43.
- 366 7. Trivedi VL, Soni R, Dhyani P, Sati P, Tejada S, Sureda A, Setzer WN, Faizal Abdull Razis A, Modu
- 367 B, Butnariu M: **Anti-cancer properties of boswellic acids: mechanism of action as anti-**
- 368 **cancerous agent.** *Frontiers in pharmacology* 2023, **14**:1187181.

8. Roy NK, Parama D, Banik K, Bordoloi D, Devi AK, Thakur KK, Padmavathi G, Shakibaei M, Fan L, Sethi G: **An update on pharmacological potential of boswellic acids against chronic diseases.** *International journal of molecular sciences* 2019, **20**(17):4101.
9. **Biopharmaceutics Classification System (BCS) of Various Drug Substance**
[<https://web.pharmacyboardkenya.org/download/biopharmaceutics-classification-system-bcs-of-various-drug-substance/>]
10. Papich MG, Martinez MN: **Applying biopharmaceutical classification system (BCS) criteria to predict oral absorption of drugs in dogs: challenges and pitfalls.** *The AAPS journal* 2015, **17**:948-964.
11. Ale-Ahmad A, Kazemi S, Daraei A, Sepidarkish M, Moghadamnia AA, Parsian H: **pH-sensitive nanoformulation of acetyl-11-keto-beta-boswellic acid (AKBA) as a potential antiproliferative agent in colon adenocarcinoma (in vitro and in vivo).** *Cancer Nanotechnology* 2024, **15**(1):49.
12. Sharma T, Jana S: **Investigation of molecular properties that influence the permeability and oral bioavailability of major β -boswellic acids.** *European Journal of Drug Metabolism and Pharmacokinetics* 2020, **45**(2):243-255.
13. Meenu M, Saurabh S, Arun N, Munish G: **Nanotechnologies for Boswellic Acids.** *American Journal of Drug Discovery and Development* 2014, **4**(1):1-11.
14. Bonilla-Vidal L, Świtalska M, Espina M, Wietrzyk J, García ML, Souto EB, Gliszczyńska A, Sánchez López E: **Dually Active Apigenin-Loaded Nanostructured Lipid Carriers for Cancer Treatment.** *International journal of nanomedicine* 2023:6979-6997.
15. Jaiswal M, Dudhe R, Sharma P: **Nanoemulsion: an advanced mode of drug delivery system.** *3 Biotech* 2015, **5**:123-127.
16. Yousefpoor Y, Amani A, Divsalar A, Vafadar MR: **Topical delivery of bee venom through the skin by a water-in-oil nanoemulsion.** *Nanomedicine Journal* 2022, **9**(2):131-137.
17. Iram F, Khan SA, Husain A: **Phytochemistry and potential therapeutic actions of Boswellic acids: A mini-review.** *Asian Pacific journal of tropical biomedicine* 2017, **7**(6):513-523.
18. Ghiasi Z, Esmaeli F, Aghajani M, Ghazi-Khansari M, Faramarzi MA, Amani A: **Enhancing analgesic and anti-inflammatory effects of capsaicin when loaded into olive oil nanoemulsion: An in vivo study.** *International Journal of Pharmaceutics* 2019, **559**:341-347.
19. Yousefpoor Y, Baharifar H, Esnaashari SS, Gheybi F, Mehrabi M, Osanloo M, Shirshahi V, Amani A: **A review of topical micro-and nanoemulsions for common skin diseases.** *Nanomedicine Journal* 2024, **11**(3).
20. Kumar M, Chawla PA, Faruk A, Chawla V: **Solid self-nanoemulsifying drug delivery systems of nimodipine: development and evaluation.** *Future Journal of Pharmaceutical Sciences* 2024, **10**(1):87.
21. Azeem A, Rizwan M, Ahmad FJ, Khar RK, Iqbal Z, Talegaonkar S: **Components screening and influence of surfactant and cosurfactant on nanoemulsion formation.** *Current Nanoscience* 2009, **5**(2):220-226.
22. No IM: **4, Introduction to Cosmetic Emulsions and Emulsification.** *Published by Micelle Press* 1997, **12**:16.
23. Na Nan S, Luckanagul JA, Panapisal VR: **The Impact of Surfactant Structures and High-Speed Mixing Dynamics in Achieving Nano-Sized Emulsions with Simple High-Speed Homogenization.** *Nanotechnology, Science and Applications* 2024:273-288.
24. Smail SS, Ghareeb MM, Omer HK, Al-Kinani AA, Alany RG: **Studies on surfactants, cosurfactants, and oils for prospective use in formulation of ketorolac tromethamine ophthalmic nanoemulsions.** *Pharmaceutics* 2021, **13**(4):467.
25. Widyaningrum I, Triyoga EF, Wibisono N, Kusumawati S, Widiyana AP: **Type of Cosurfactant Effects on Particle Size in Nanoemulsion Drug Delivery Systems.** *East Asian Journal of Multidisciplinary Research* 2023, **2**(9):3811-3820.

- 419 26. Liao W, Gharsallaoui A, Dumas E, Ghnimi S, Elaissari A: **Effect of carrier oil on the properties**
420 **of sodium caseinate stabilized O/W nanoemulsions containing Trans-cinnamaldehyde.** *Lwt*
421 2021, **146**:111655.
- 422 27. Wooster TJ, Golding M, Sanguansri P: **Impact of oil type on nanoemulsion formation and**
423 **Ostwald ripening stability.** *Langmuir* 2008, **24**(22):12758-12765.
- 424 28. Sabzalizade S, Amani A, Vatandoost H, Hosseini F, Najafi-Taher R, Basseri HR: **Evaluation of**
425 **Nanoemulsion of Eucalyptus globulus Oil as Potent Botanical Larvicide against Malaria**
426 **Vector, Anopheles stephensi and West Nile Vector, Culex pipiens Under Laboratory and**
427 **Semi-Field Conditions.** *Journal of Arthropod-Borne Diseases* 2021, **15**(4):380-388.
- 428 29. Sessa M, Balestrieri ML, Ferrari G, Servillo L, Castaldo D, D'Onofrio N, Donsi F, Tsao R:
429 **Bioavailability of encapsulated resveratrol into nanoemulsion-based delivery systems.** *Food*
430 *chemistry* 2014, **147**:42-50.
- 431 30. Krüger P, Kanzer J, Hummel J, Fricker G, Schubert-Zsilavecz M, Abdel-Tawab M: **Permeation**
432 **of Boswellia extract in the Caco-2 model and possible interactions of its constituents KBA**
433 **and AKBA with OATP1B3 and MRP2.** *European journal of pharmaceutical sciences* 2009,
434 **36**(2-3):275-284.
- 435 31. Sharma T, Jana S: **Investigation of molecular properties that influence the permeability and**
436 **oral bioavailability of major β -boswellic acids.** *European Journal of Drug Metabolism and*
437 *Pharmacokinetics* 2020, **45**:243-255.
- 438 32. Rebouças LM, Sousa AC, Gramosa NV, Araújo TGd, Oliveira FdCEd, Pessoa CdÓ, Araújo RS,
439 Santos E, Ricardo NM: **Linseed Oil Nanoemulsion with Pluronic® F127 Loaded with Betulinic**
440 **Acid: Preparation, Rheology, MTT Assay and in vitro Release Kinetics.** *Journal of the*
441 *Brazilian Chemical Society* 2022, **33**:1319-1331.
- 442 33. Fraga M, Laux M, Rejane dos Santos G, Zandona B, Dos Santos Giuberti C, De Oliveira M, da
443 Silveira Matte U, Ferreira Teixeira H: **Evaluation of the toxicity of oligonucleotide/cationic**
444 **nanoemulsion complexes on Hep G2 cells through MTT assay.** *Die Pharmazie-An*
445 *international journal of pharmaceutical sciences* 2008, **63**(9):667-670.
- 446 34. Liu D-Z, Lecluyse EL, Thakker DR: **Dodecylphosphocholine-mediated enhancement of**
447 **paracellular permeability and cytotoxicity in Caco-2 cell monolayers.** *Journal of*
448 *pharmaceutical sciences* 1999, **88**(11):1161-1168.
- 449 35. Hubatsch I, Ragnarsson EG, Artursson P: **Determination of drug permeability and prediction**
450 **of drug absorption in Caco-2 monolayers.** *Nature protocols* 2007, **2**(9):2111-2119.
- 451 36. Piazzini V, Monteforte E, Luceri C, Bigagli E, Bilia AR, Bergonzi MC: **Nanoemulsion for**
452 **improving solubility and permeability of Vitex agnus-castus extract: formulation and in**
453 **vitro evaluation using PAMPA and Caco-2 approaches.** *Drug delivery* 2017, **24**(1):380-390.
- 454 37. Faassen F, Kelder J, Lenders J, Onderwater R, Vromans H: **Physicochemical properties and**
455 **transport of steroids across Caco-2 cells.** *Pharmaceutical research* 2003, **20**:177-186.
- 456 38. Yang Y, Zhao Y, Yu A, Sun D, Yu L: **Oral drug absorption: Evaluation and prediction.** In:
457 *Developing solid oral dosage forms.* Elsevier; 2017: 331-354.
- 458 39. Lapa G: **Molecular-biological problems of drug design and mechanism of drug action: Triple**
459 **inhibitors of monoamine reuptake transporters: first results and outlook.** *Pharmaceutical*
460 *Chemistry Journal* 2011, **45**(6):323-328.
- 461 40. Ketabchi N, Esmaeili F, Amani A: **Pharmacokinetic Characteristics and Therapeutic Efficacy of**
462 **Frankincense Extract Nanoemulsion on Multiple Sclerosis: An Animal Study.**
463 *BioNanoScience* 2025, **15**(3):1-15.
- 464 41. Boyd J, Parkinson C, Sherman P: **Factors affecting emulsion stability, and the HLB concept.**
465 *Journal of Colloid and Interface Science* 1972, **41**(2):359-370.
- 466 42. Brunaugh AD, Smyth HD, Williams III RO, Brunaugh AD, Smyth HD, Williams III RO: **Disperse**
467 **systems: emulsions.** *Essential Pharmaceuticals* 2019:111-121.

43. Karakocak BB, Keshavan S, Gunasingam G, Angeloni S, Auderset A, Petri-Fink A, Rothen-Rutishauser B: **Rethinking of TEER measurement reporting for epithelial cells grown on permeable inserts.** *European Journal of Pharmaceutical Sciences* 2023, **188**:106511.
44. Ci X-Y: **Absorption of 3-acetyl-11-keto- β -boswellic acid in Caco-2 cells and MDCK cell models.** *Chinese Traditional and Herbal Drugs* 2013:1162-1167.
45. Kou L, Bhutia YD, Yao Q, He Z, Sun J, Ganapathy V: **Transporter-guided delivery of nanoparticles to improve drug permeation across cellular barriers and drug exposure to selective cell types.** *Frontiers in pharmacology* 2018, **9**:27.
46. Mushtaq A, Wani SM, Malik A, Gull A, Ramniwas S, Nayik GA, Ercisli S, Marc RA, Ullah R, Bari A: **Recent insights into Nanoemulsions: Their preparation, properties and applications.** *Food Chemistry: X* 2023:100684.
47. Çınar K: **A review on nanoemulsions: preparation methods and stability.** *Trakya Üniversitesi Mühendislik Bilimleri Dergisi* 2017.
48. Alberts B, Johnson A, Lewis J, Raff M, Roberts K, Walter P: **Cell junctions.** In: *Molecular Biology of the Cell 4th edition.* Garland Science; 2002.
49. Stürner KH, Stellmann J-P, Dörr J, Paul F, Friede T, Schammler S, Reinhardt S, Gellissen S, Weissflog G, Faizy TD: **A standardised frankincense extract reduces disease activity in relapsing-remitting multiple sclerosis (the SABA phase IIa trial).** *Journal of Neurology, Neurosurgery & Psychiatry* 2018, **89**(4):330-338.
50. Ammon H: **Boswellic acids in chronic inflammatory diseases.** *Planta medica* 2006, **72**(12):1100-1116.
51. Hüsch J, Bohnet J, Fricker G, Skarke C, Artaria C, Appendino G, Schubert-Zsilavecz M, Abdel-Tawab M: **Enhanced absorption of boswellic acids by a lecithin delivery form (Phytosome®) of Boswellia extract.** *Fitoterapia* 2013, **84**:89-98.
52. Vijayarani KR, Govindarajulu M, Ramesh S, Alturki M, Majrashi M, Fujihashi A, Almaghrabi M, Kirubakaran N, Ren J, Babu RJ: **Enhanced bioavailability of boswellic acid by Piper longum: a computational and pharmacokinetic study.** *Frontiers in Pharmacology* 2020, **11**:551911.
53. Meins J, Behnam D, Abdel-Tawab M: **Enhanced absorption of boswellic acids by a micellar solubilized delivery form of Boswellia extract.** *NFS J* **11**: 12–16. In.; 2018.
54. Khani S, Keyhanfar F, Amani A: **Design and evaluation of oral nanoemulsion drug delivery system of mebudipine.** *Drug delivery* 2016, **23**(6):2035-2043.
55. Azami SJ, Amani A, Keshavarz H, Najafi-Taher R, Mohebbali M, Faramarzi MA, Mahmoudi M, Shojaee S: **Nanoemulsion of atovaquone as a promising approach for treatment of acute and chronic toxoplasmosis.** *European Journal of Pharmaceutical Sciences* 2018, **117**:138-146.
56. Stuchlík M, Zak S: **Lipid-based vehicle for oral drug delivery.** *Biomedical Papers-Palacky University in Olomouc* 2001, **145**(2):17-26.
57. Shaker DS, Ishak RA, Ghoneim A, Elhuoni MA: **Nanoemulsion: A review on mechanisms for the transdermal delivery of hydrophobic and hydrophilic drugs.** *Scientia Pharmaceutica* 2019, **87**(3):17.
58. Aburahma MH, El-Laithy HM, Hamza YE-S: **Oral bioavailability enhancement of vinpocetine using self-microemulsifying drug delivery system containing long chain triglycerides: Preparation and in vitro/in vivo evaluation.** *Clinical Research and Regulatory Affairs* 2010, **27**(4):97-107.
59. Gershanik T, Benita S: **Self-dispersing lipid formulations for improving oral absorption of lipophilic drugs.** *European journal of pharmaceuticals and biopharmaceutics* 2000, **50**(1):179-188.

517 **Graphical Abstract:**



518

519 3-Acetyl-11-keto-β-boswellic acid (AKBA) shows promise for treating inflammatory and
 520 cancer-related disorders; however, its low oral bioavailability limits its effectiveness. This study
 521 developed a nanoemulsion (NE) delivery system for AKBA, resulting in a particle size of 12–15
 522 nm that improved transport in Caco-2 cells. In vivo, C_{max} increased from 3.36 to 12.23 μg/mL,
 523 and AUC_{0-t} rose from 4257 to 6222 μg·h/mL, with T_{max} at 6 h. NE significantly enhances AKBA's
 524 bioavailability.